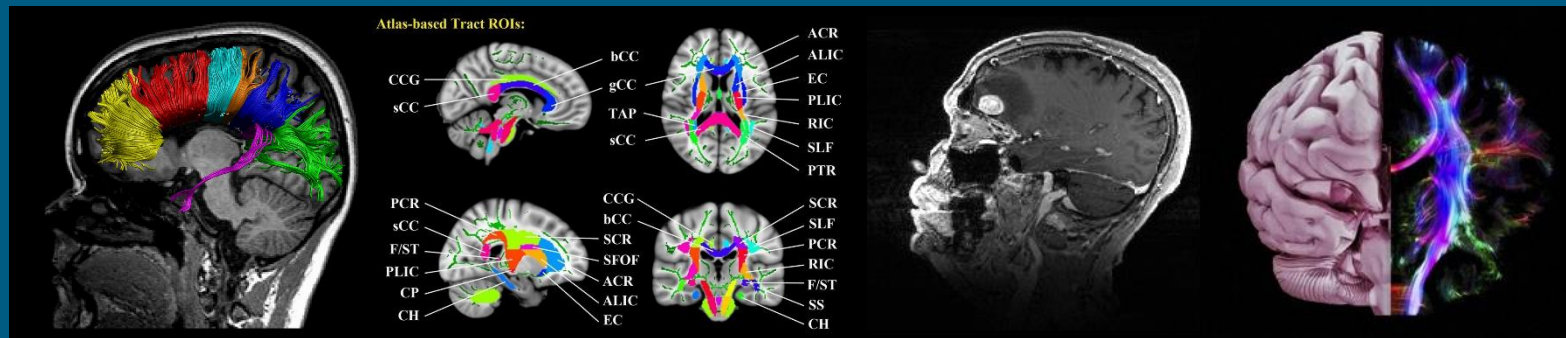


My experience in Juelich as a master student

Development and Applications of Novel Diffusion MRI Biomarkers in Neurology



Ana Gogishvili

Supervisors:

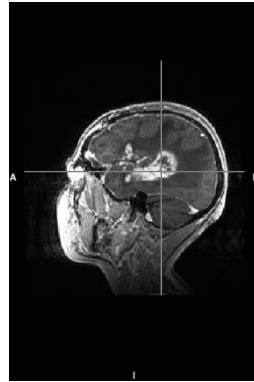
Priv. – Doz. Dr. Farida Grinberg

Prof. Dr. Ketevan Kotetishvili

Prof. Dr. N. J. Shah



GGSWBS'14
July 2014



Julich
Internship: INM-4

Julich
Internship: INM-4



Feb – Aug
2018

Julich
Internship: INM-4



Autumn lectures
2015

GGSWBS'16



Julich
Master defense: INM-4

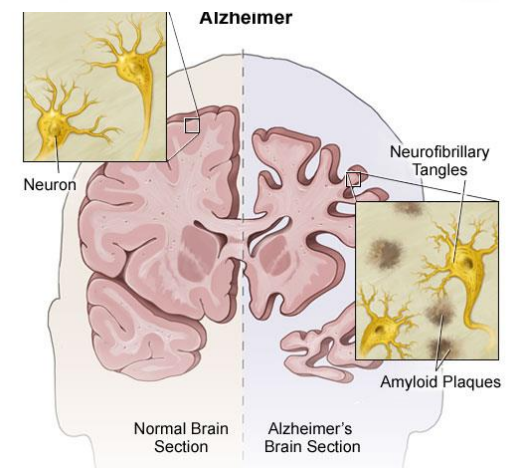
Outline

- Introduction (DTI, DKI)
- Applications: Gamma distribution function metrics as biomarker of maturation
- Multimodal Study of Brain Tumors

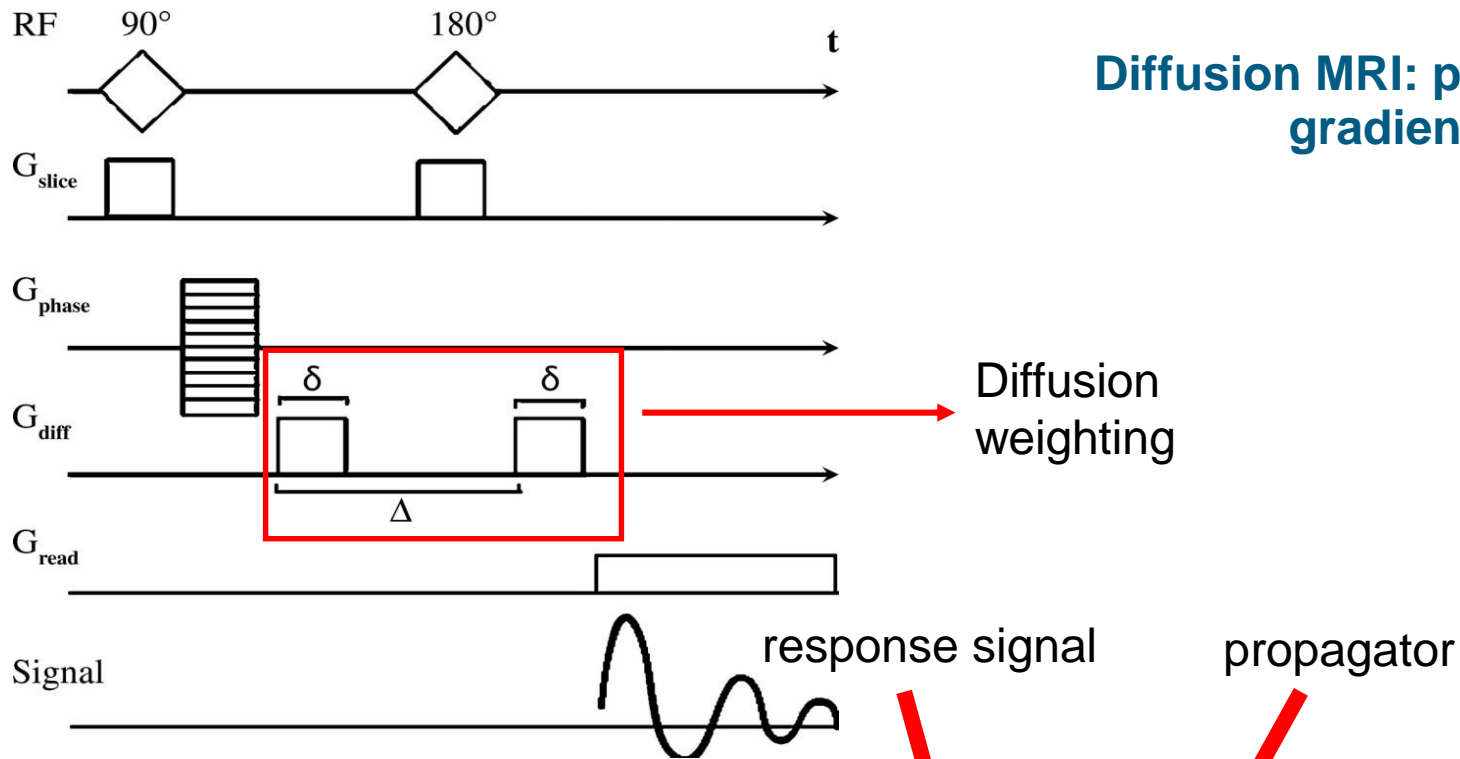
Introduction

Diffusion MRI applications:

- neurodegenerative pathologies (Alzheimer's and Parkinson's diseases, etc.)
- stroke
- neurosurgical planning
- development and aging
- tumours



Water Diffusion is random, microscopic movement due to thermal collisions

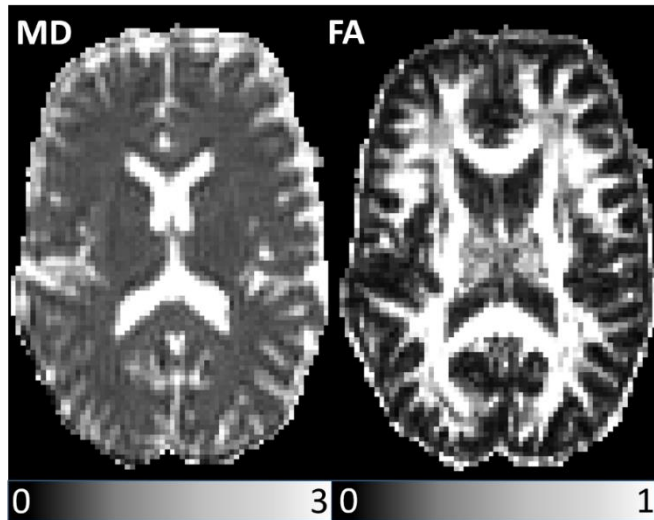


Diffusion MRI: pulsed field gradients

Diffusion weighting

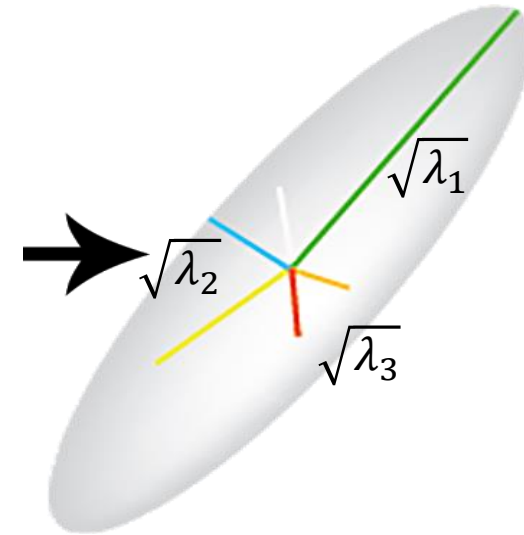
$$\Psi_{diff} = \int P(z, t) e^{i\gamma G \delta z} dz$$

Diffusion tensor imaging: accounts for diffusion anisotropy



Signal attenuation

$$S(\mathbf{b}) = S_0 e^{-\mathbf{b}_{ij} D_{ij}}$$



Tensor invariants:

Fractional Anisotropy

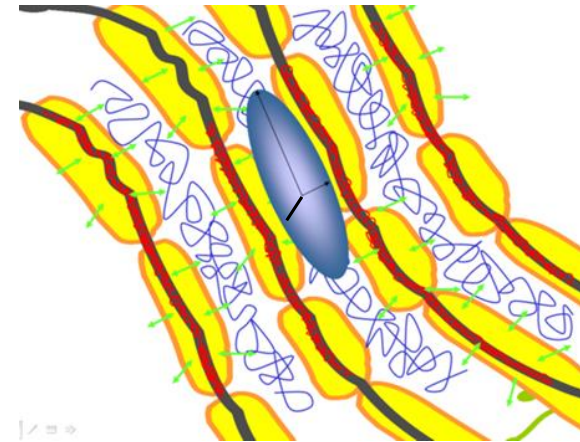
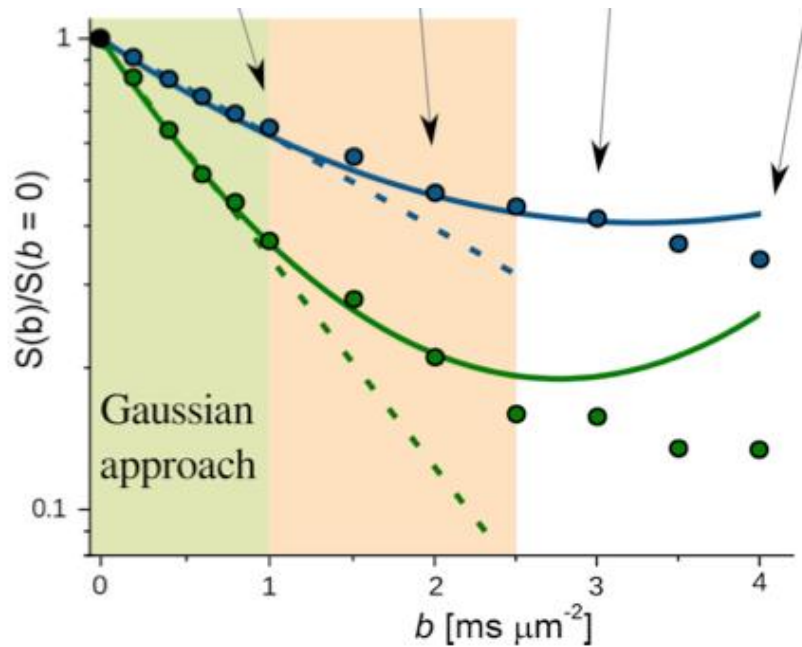
$$FA = \sqrt{\frac{3}{2}} \sqrt{\frac{(MD - l_1)^2 + (MD - l_2)^2 + (MD - l_3)^2}{l_1^2 + l_2^2 + l_3^2}}$$

Mean Diffusivity

$$MD = \frac{l_1 + l_2 + l_3}{3}$$

Introduction

Non-gaussian Diffusion Kurtosis Imaging (DKI)



Water diffusion is anisotropic and restricted

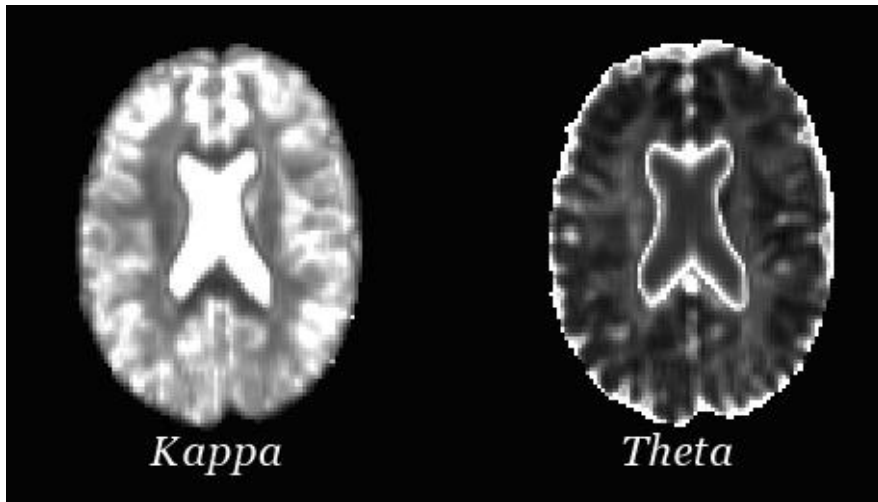
$$\ln \frac{S(b)}{S_0} = \underbrace{-bD_K}_{\text{Monoexponential}} + \frac{1}{6} \underbrace{(bD_K)^2 K}_{\text{Non-exponential}} + \mathcal{O}(b^3)$$

Mean kurtosis:

$$MK \equiv \frac{1}{5} \text{Tr}(\mathbf{K}) = \langle \mathbf{K} \rangle$$

Non- Gaussian method: Gamma Distribution Function Imaging

F. Grinberg et al., PLOS ONE, 2014



$$S(b) = \int_0^\infty P(D) \exp(-bD) dD$$

$$P_G(D, \kappa, \theta) = D^{\kappa-1} \frac{\exp(-D/\theta)}{\Gamma(\kappa)\theta^\kappa}$$

Free parameters

$$\text{Kappa: } \kappa = \langle D \rangle^2 / \sigma_G^2$$

$$\text{Theta: } \theta = \sigma_G^2 / \langle D \rangle$$

Application of Gamma Distribution function to children and adults

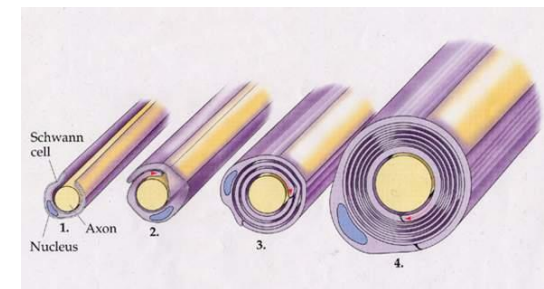
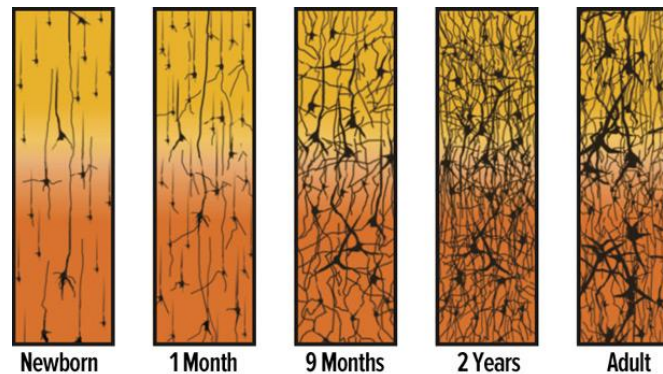
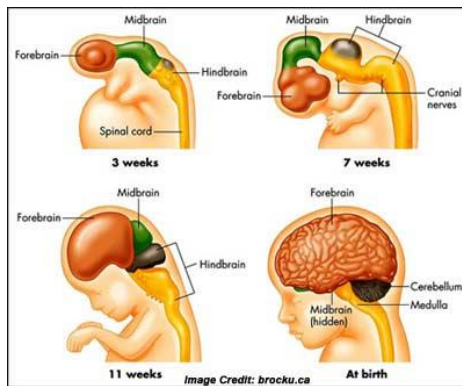
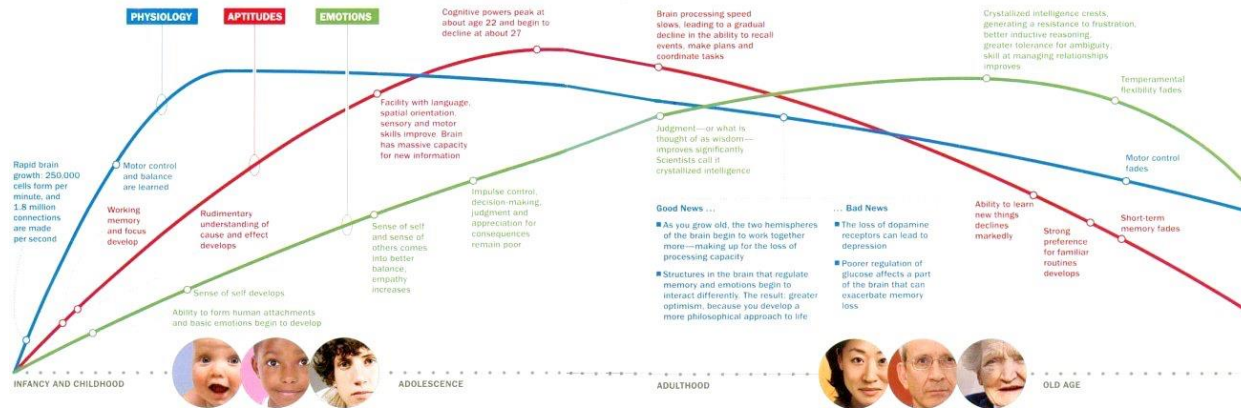
In particular we are interested Following questions...

1. Are the GDF parameters efficient in tracking the differences between children and adults?
2. Can we extend our knowledge about more subtle microstructural development of specific fibres based on GDF?

Diffusion kurtosis metrics as biomarkers of microstructural development: A comparative study of a group of children and a group of adults

F. Grinberg et al., Neuroimage, 2017

Brain Development and Ageing – Lifelong Changes



Human brain undergoes life-long changes in many aspects: anatomic, physiological, mental, and also microstructural. Typical trajectories of the changes are often U-shaped or inverted-U-shaped.

Two groups for comparison children and adults

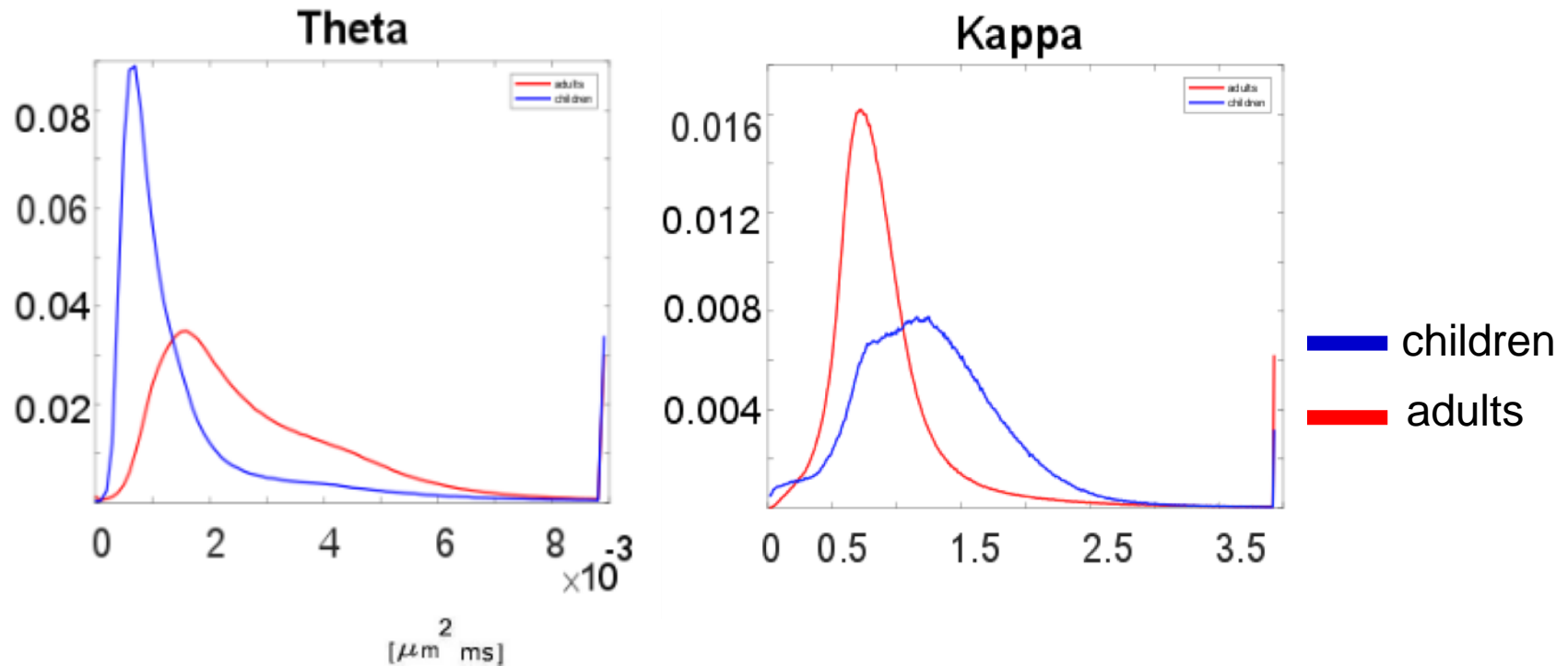
Children
n=20
(9-12) years



Adults
n=21
(38-64) years

whole-body 3T Siemens MAGNETOM Tim-Trio scanner

Averaged histograms



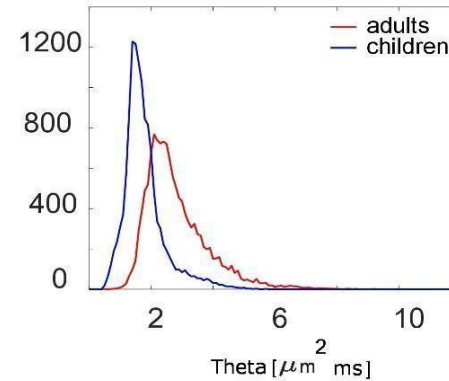
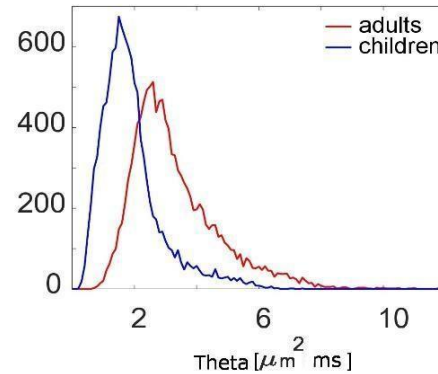
Whole brain averaged histograms show large shifts between the group of children and the group of adults

Regional analysis in white matter

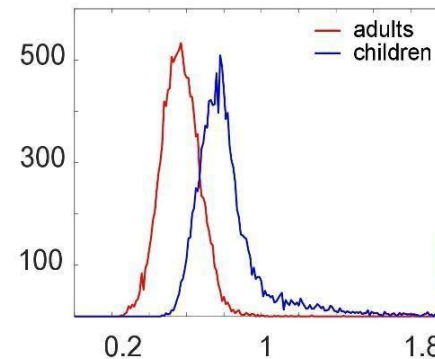
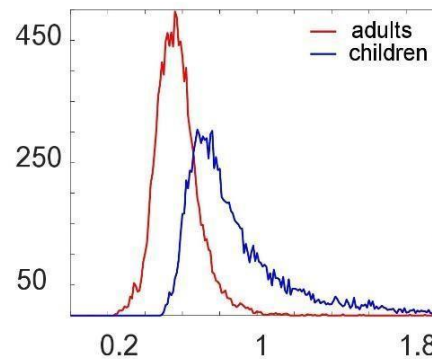
Sagittal Stratum

Retrolenticular part internal capsule

Theta



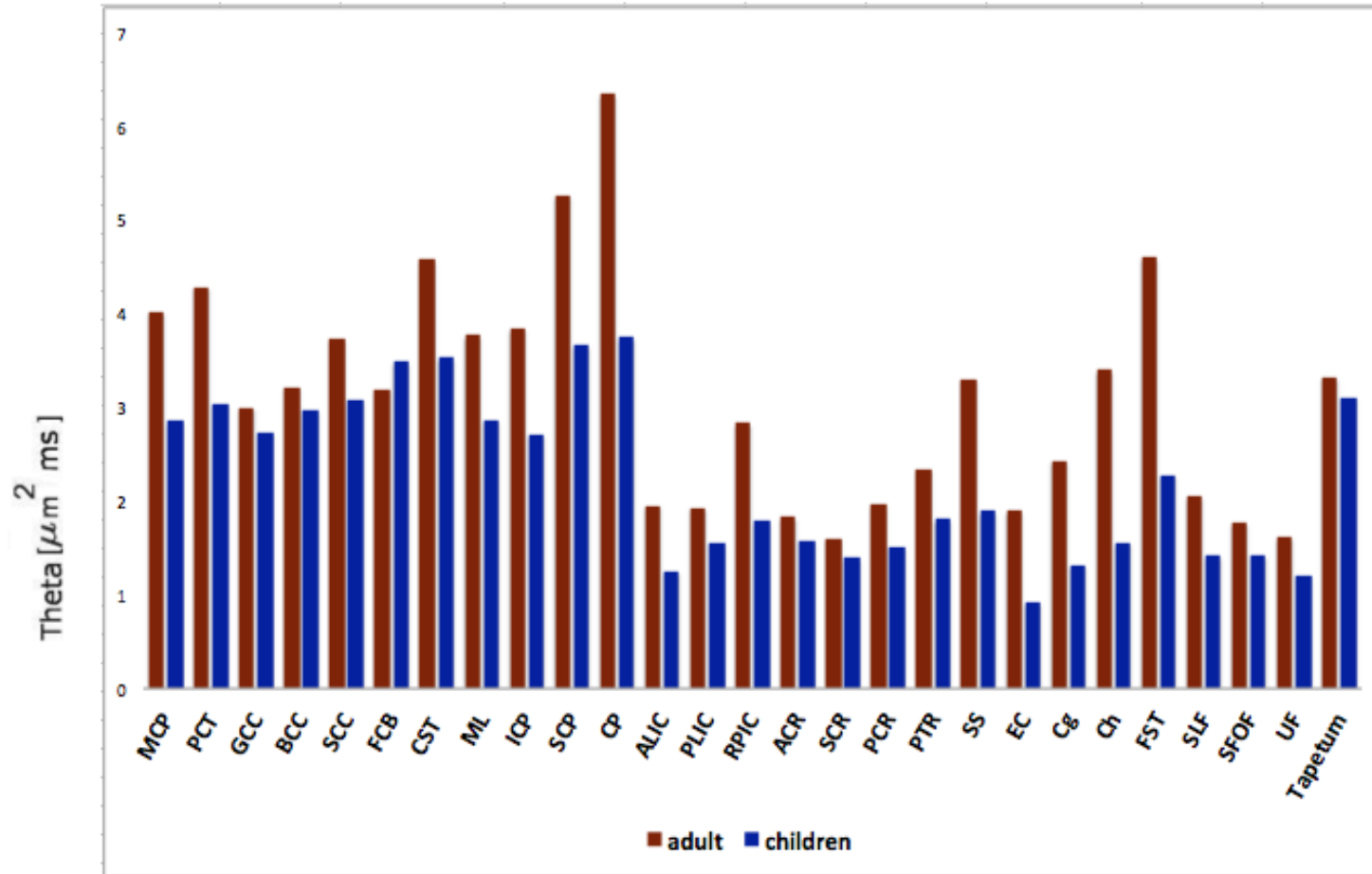
Kappa



Regional analysis shows large shifts for various fibers

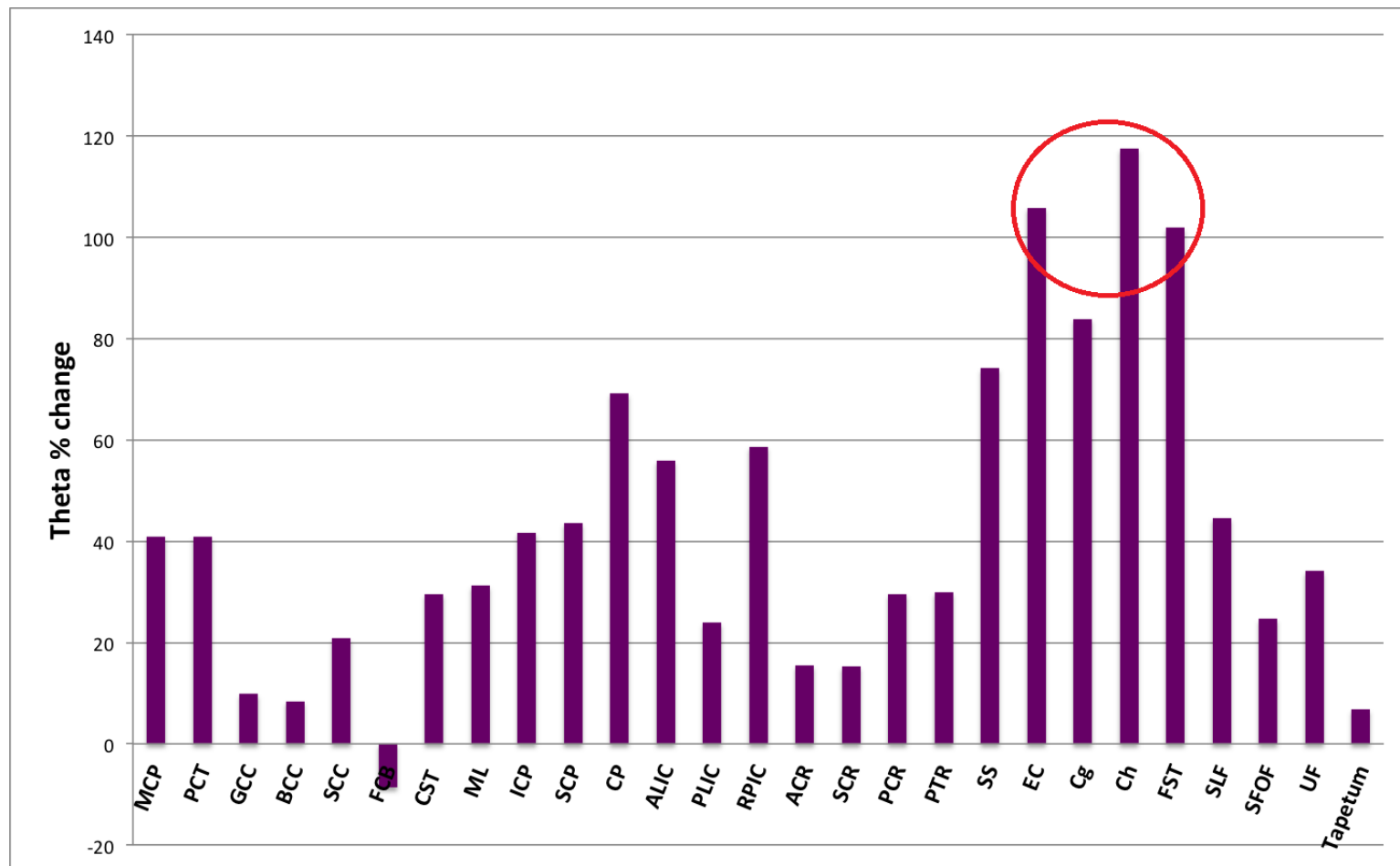
Regional Analysis

Differences between the mean values of theta in various region



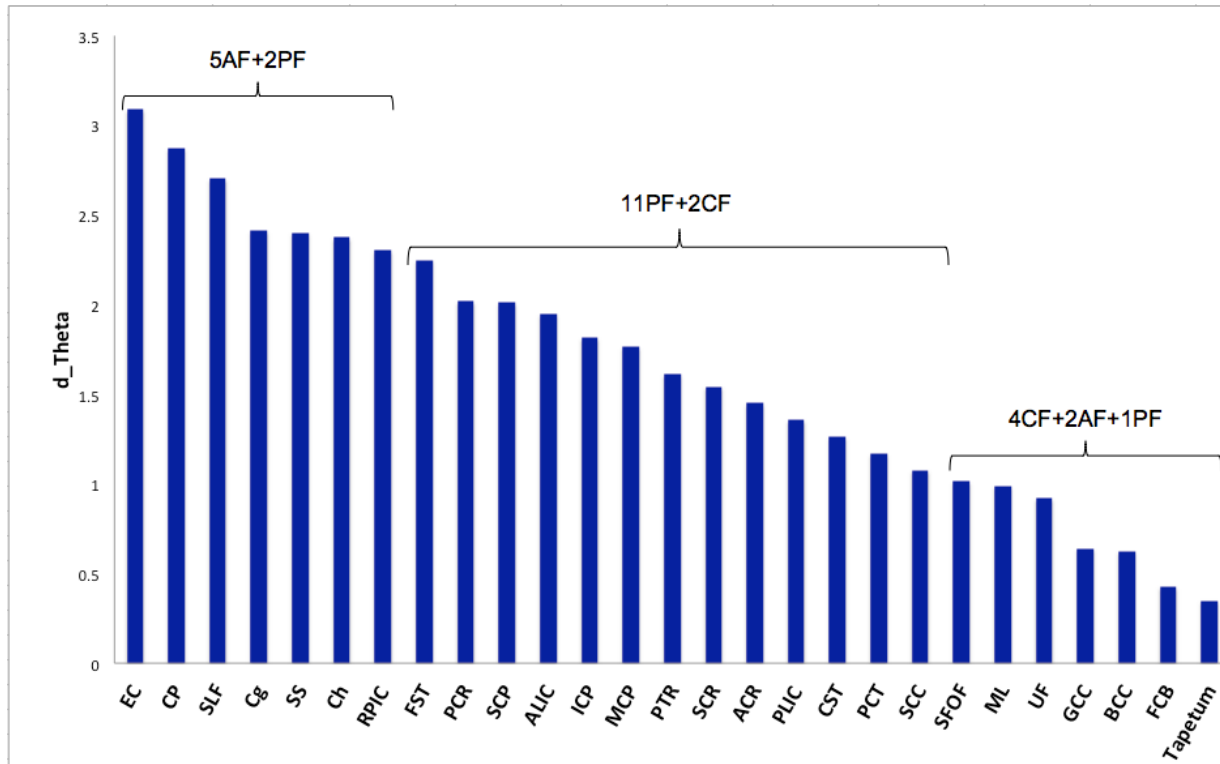
Theta values are larger in adults than children in all fibres

Group differences in percentage for Theta parameter



Fibre ranking based on Cohen's d of Theta

Protracted maturation



1st quartile:
All 4 CFs+2 AFs+1 PFs

2 middle quartile
between:1st and 4th
quartiles
All 1 PFs+2CFs

4th quartiles:
All 5 AFs+ 2 PFs

Cohen's d (effect size):

$$d = \frac{M_1 - M_2}{SD_{pooled}}$$

≈ 0.2 - 'small'

≈ 0.5 - 'medium'

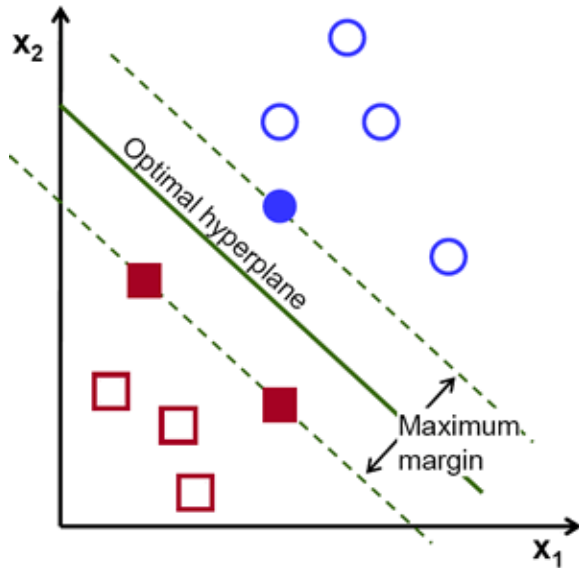
≈ 0.8 - 'large'

> 1.2 - 'very large'

7 association fibres
14 Projection fibres
6 Commissural Fibres

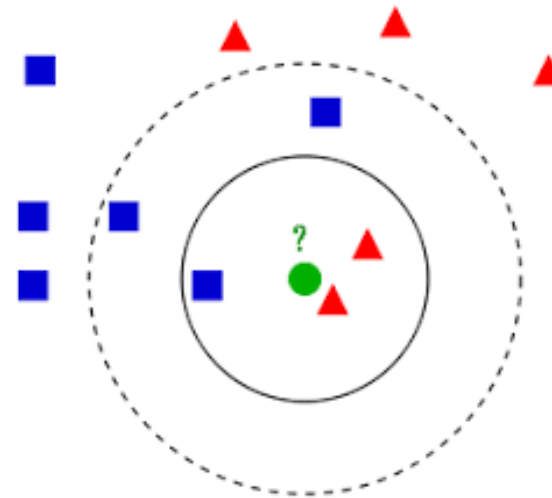
Classifiers: Support Vector Machine and k Nearest Neighbour algorithm

SVM



SVM algorithm is based on finding the hyper plane that gives the largest minimum distance to the training examples

kNN



An object is classified by a majority vote of its neighbors, with the object being assigned to the class most common among its k nearest neighbors

Normalization of feature vector:
$$X'_i = \frac{X_i - X_{min}}{X_{max} - X_{min}}$$

Classification based on DTI and GDF metrics of different regions

Accuracies of classification (Alpha=0.01)

	FA	MD	AD	RD	Kappa	Theta	DG	sG
SVM	0.89	0.94	0.95	0.76	0.99	0.73	0.87	0.95
kNN	0.87	0.91	0.92	0.78	0.99	0.76	0.92	0.97
k	3	5	3	5	1	1	3	3



DTI



GDF

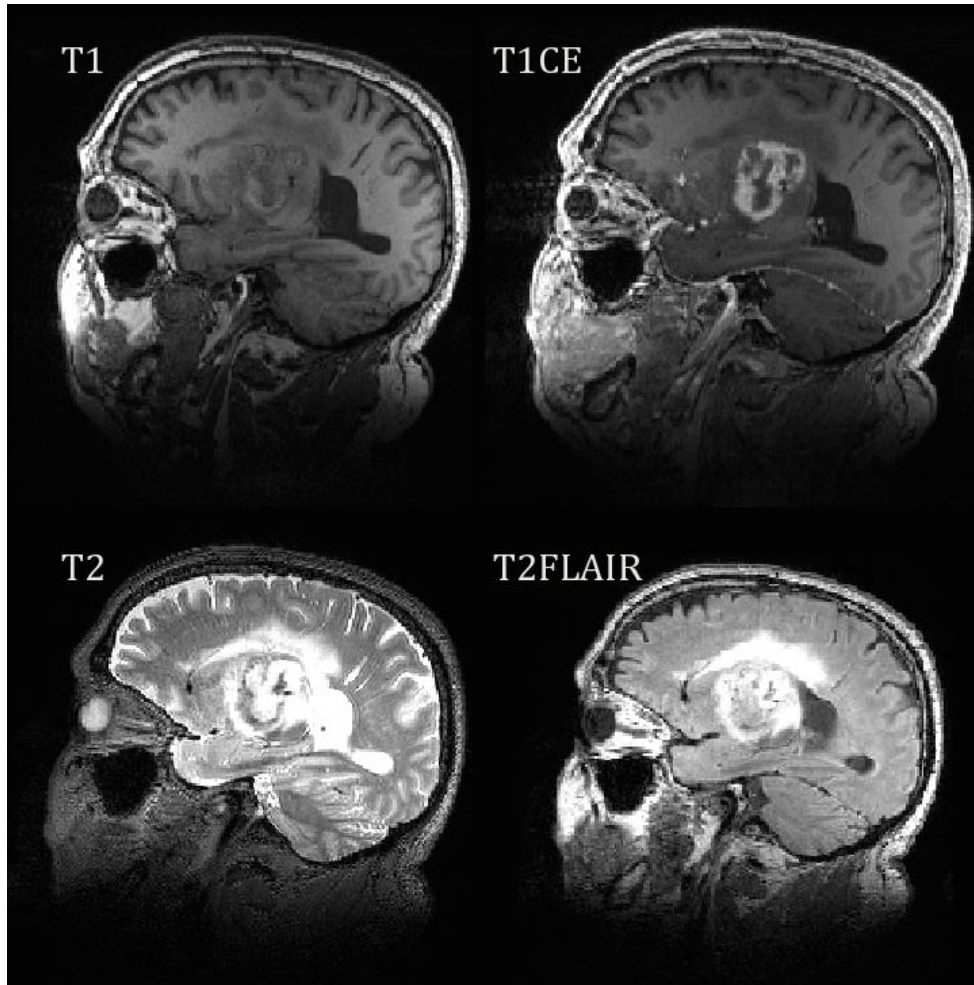
All metrics have shown high accuracies

Summary of first part

Gamma distribution function provides promising complementary metrics to a palette of maturation -sensitive MRI tools.

Tumour

24 untreated tumour patient
Whole body 3T Siemens MAGNETOM Tim-Trio scanner



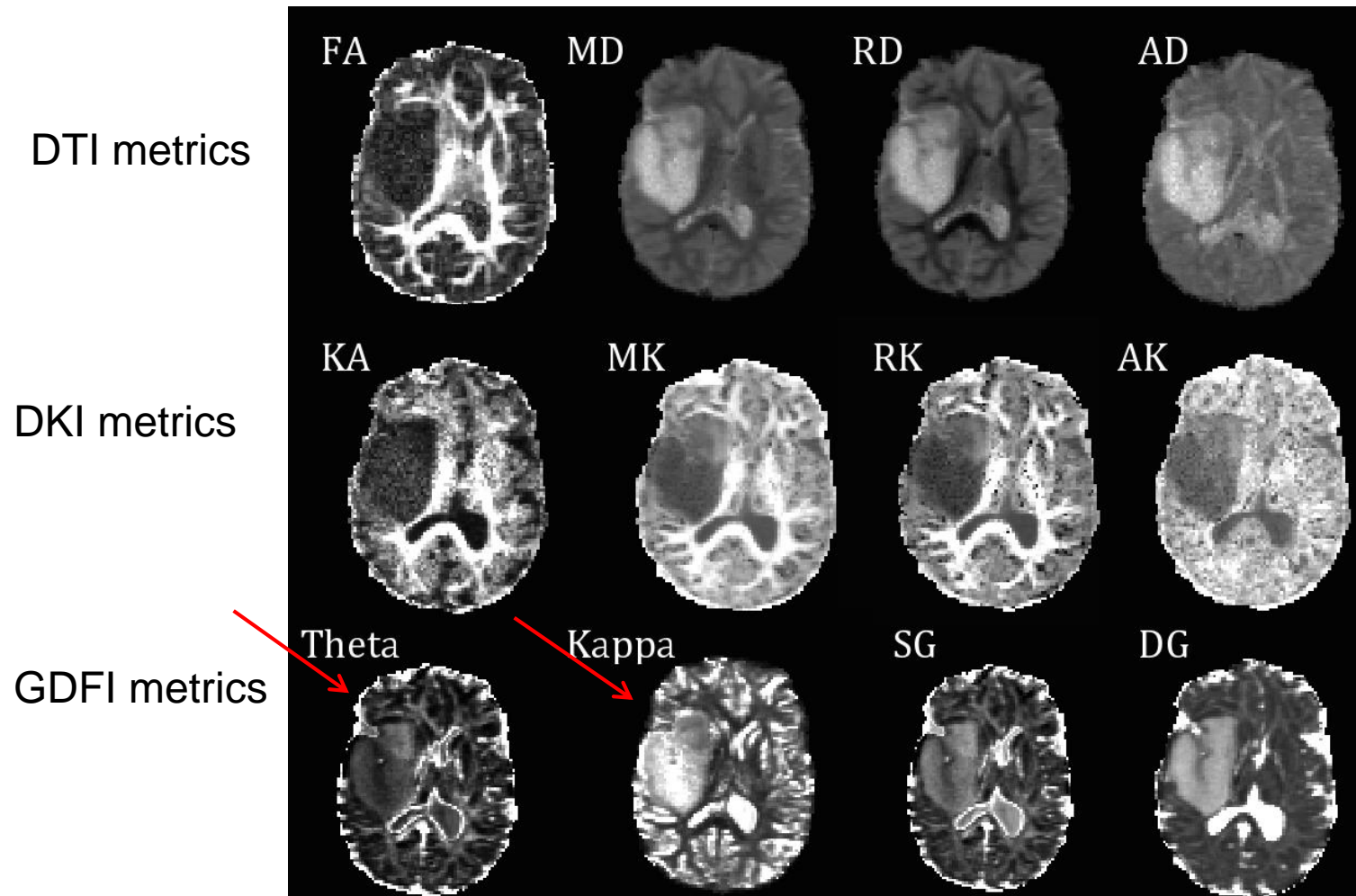
T1-weighted images

**T1-weighted images with
contrast enhanced**

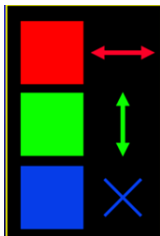
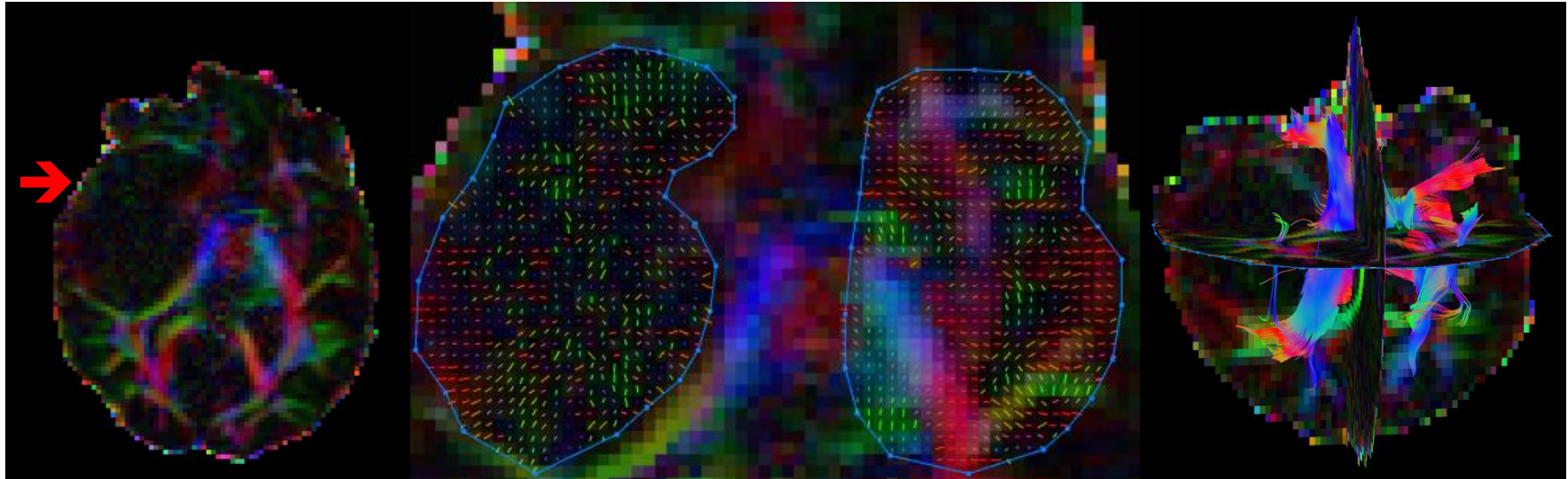
T2-weighted image

**T2FLAIR (Fluid attenuated
Inversion Recovery)**

Diffusion parameters



Color-encoded FA and fiber tracking for a tumor human brain in axial plane



Diffusion MRI gives a lot of complementary information to tumor assessment

This project is on going process and future work provide more results!

Conclusions

- Novel diffusion models provide information about tissue conditions, which is not attainable with conventional DMRI.
- The results show the efficiency of the gamma parameters, it can show the tumor heterogeneity
- All non-Gaussian models shown to provide valuable information regarding the tissue microstructure and conditions.

Acknowledgements

- Dr. Farida Grinberg
- Dr. Ezequiel Farrher
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**Thank you
for
your attention !**